

**SYSTEM AND METHOD FOR BIOAEROSOL DISCRIMINATION BY
TIME-RESOLVED FLUORESCENCE**

RELATED APPLICATION

5 This application claims priority under 35 U.S.C. § 119(e) to U.S. Provisional Application Serial No. 60/453,325, entitled "Method for Bioaerosol Discrimination by Time-Resolved Laser Induced Fluorescence (TRILIF)," filed on March 10, 2003, which is herein incorporated by reference in its entirety.

10 **FEDERALLY SPONSORED RESEARCH**

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BACKGROUND OF INVENTION

15 1. Field of Invention

 The present invention relates to classifying particles and, in particular, to utilizing time-based fluorescence techniques to characterize the biological nature of aerosol particles.

20 2. Discussion of Related Art

 Detection of biological aerosol particles or bioaerosols can be important in many fields including, for example, agriculture, food processing, public health, worker safety, resident/patient safety, disease prevention and eradication, emergency response, homeland defense and counterterrorism, and military base and force
25 protection because bioaerosols may be harmful to human or animal health. Intrinsic particle fluorescence is a method that be utilized to distinguish biological particles from non-biological background particles. However, atmospheric pollutants may also fluoresce and can cause fluorescence-based instruments to register false positive
30 indications. Various systems and methods can be utilized to characterize the nature of aerosol particles. For example, common detectors, cue detectors or trigger detectors, are typically optical scattering particle counters equipped with laser-induced

fluorescence detection devices. Typically in such a system, an ultraviolet laser beam excites a particle to be examined. The particle's resultant fluorescence can be dispersed into two detection channels, roughly divided between ultraviolet and visible wavelengths. The particle is thereafter classified as threatening or non-threatening according to its relative position on a three-dimensional graph of UV intensity, visible intensity, and scattering intensity. While progress has been made these detectors still suffer from potential interference due to background fluorescence.

For example, Brewer, in U.S. Patent No. 3,566,114, discloses a method and means for detection of microorganisms in the atmosphere. Macias et al., in U.S. Patent No. 4,013,888, disclose a monitor for atmospheric pollutants. Javan, in U.S. Patent No. 4,561,010, discloses a method and apparatus for fluorescent sensing. Hirako et al., in U.S. Patent No. 5,158,889, disclose a biological cell sorter. Ho, in U.S. Patent Nos. 5,701,012 and 5,895,922, discloses fluorescent biological particle detection systems. Gillespie et al., in U.S. Patent No. 5,828,452, disclose a spectroscopic system with a single converter and method for removing overlay in time of detected emissions. Zborowski et al., in U.S. Patent No. 6,142,025, disclose a method for determining particle characteristics. Fukuda et al., in U.S. Patent No. 6,165,740, disclose a method and device for flow-cytometric microorganism analysis. Jeys et al., in U.S. Patent No. 6,194,731, disclose a bio-particle fluorescence detector. Ray et al., in U.S. Patent No. 6,608,677, disclose a mini-LIDAR sensor for the remote stand-off sensing of chemical/biological substances and methods for sensing same. Simonson et al., in U.S. Patent No. 6,617,591, disclose a method for remote detection of trace contaminants. Carrión et al., in U.S. Patent No. 6,630,299, disclose fluorescence detection. Gillispie, in U.S. Patent Application Publication 2002/0158211, disclose a multi-dimensional fluorescence apparatus and method for rapid and highly sensitive quantitative analysis of mixtures.

SUMMARY OF INVENTION

In accordance with one or more embodiments, the present invention relates to a system for classifying aerosol particles. The system can comprise a detector capable of generating a signal corresponding to a composite emission decay profile of an

emission from an aerosol particle and a means for deconvolving the signal into a discriminant vector that provides an indication of the nature of the aerosol particle.

In accordance with one or more embodiments, the present invention relates to a system for classifying aerosol particles. The system can comprise a detector capable
5 of generating a signal corresponding to a composite emission decay profile of an emission from a sample of aerosol particles and a processor coupled to the detector to receive the signal. The processor can determine a scatter component and a fluorescence component of the composite emission decay profile.

In accordance with one or more embodiments, the present invention relates to
10 a method of classifying an aerosol particle. The method can comprise measuring a composite emission decay profile of an emission from the aerosol particle, determining a biological fluorescence time constant of the composite emission decay profile, and determining a biological emission constant of the composite emission decay profile.

In accordance with one or more embodiments, the present invention relates to
15 a method of classifying aerosol particles. The method can comprise stimulating the aerosol particles to promote radiation emission; measuring a composite emission decay profile of the radiation emission, the composite emission decay profile comprising a scatter component, a first fluorescence component, and a second
20 fluorescence component; determining a scatter emission constant corresponding to the scatter component; determining a first fluorescence emission constant of the composite emission decay profile; and determining a second fluorescence emission constant of the composite emission decay profile.

In accordance with one or more embodiments, the present invention relates to
25 a method of classifying an aerosol particle. The method can comprise measuring a composite emission from an aerosol particle, deconvolving the composite emission to determine a discriminant vector of the aerosol particle, and mapping the discriminant vector to provide an indication of the nature of the aerosol particle.

BRIEF DESCRIPTION OF DRAWINGS

The accompanying drawings, are not intended to be drawn to scale. In the drawings, each identical or nearly identical component that is illustrated in various figures is represented by a like numeral. For purposes of clarity, not every component may be labeled in every drawing. In the drawings:

FIG. 1 is a graph showing a response, exemplarily shown as a composite emission decay profile, from an aerosol particle in accordance with one or more embodiments of the present invention;

FIG. 2 is a schematic diagram showing a system in accordance with one or more embodiments of the present invention;

FIG. 3 is a schematic diagram of a flow cell utilizable in accordance with one or more embodiments of the present invention;

FIG. 4 is a graph showing components of the decay shown in FIG. 1;

FIG. 5 is map characterizing deconvolved results in accordance with one or more embodiments of the present invention;

FIG. 6 is a graph showing the relative nature of a scatter component (A), a biological fluorescence component (B), and a non-biological fluorescence component (C) of a typical decay response;

FIGS. 7A-7E are graphs showing constructed, prophetic decay responses for various particles as discussed in the examples; and

FIG. 8 is a map characterizing the nature of the various particles having responses shown in FIGS. 7A-7E and as discussed in the examples.

DETAILED DESCRIPTION

This invention is not limited in its application to the details of construction and the arrangement of components set forth in the following description or illustrated in the drawings. The invention is capable of other embodiments and of being practiced or of being carried out in various ways. Also, the phraseology and terminology used herein is for the purpose of description and should not be regarded as limiting. The use of “including,” “comprising,” or “having,” “containing,” “involving,” and

variations thereof herein, is meant to encompass the items listed thereafter and equivalents thereof as well as additional items.

Detectable fluorescent compounds include, for example, polycyclic aromatic hydrocarbons (PAHs). Typical sources of PAH species are combustion sources, including for example, internal combustion engines that utilize gasoline or diesel fuel. Such sources typically discharge PAH species on soot particles, which though small, can aggregate and grow to larger size. Some PAH species are semivolatile, and will partially evaporate into the gas phase and may re-condense on other particles. Thus, in some cases, non-fluorescent particles may become fluorescent, especially where significant concentrations of PAH species would be present. In some cases, fluorescence due to PAH condensation on non-fluorescent particles may equal or exceed that from similarly-sized biological aerosol particles. Such PAH-contaminated particles can create false conditions. For example, the detecting instrument may register a false positive when non-biological species are present; or high levels of fluorescence from non-biological species may mask fluorescence from biological species, causing a false negative. Biological molecules have typically short fluorescence lifetimes, about less than 1 to about 7 ns. In contrast, PAH species have typically much longer lifetimes, typically exceeding 7 ns, and in some cases, from 10 ns to hundreds of nanoseconds.

Biological aerosol particles can be excited to produce fluorescence from biological fluorophores such as tryptophan, tyrosine, NADH, and/or flavin compounds, which would typically be present in such bioaerosol particles. In some cases, such particles can also scatter radiation as a scattered light pulse. Said excitation event can produce a signal pulse, typically a composite emission decay profile or composite intensity, exemplarily shown in FIG. 1. The composite emission decay profile typically includes a scatter component and fluorescence from one or more of particle-bound biological fluorophores; particle-bound, non-biological organic fluorophores; and, in some cases, gas phase, non-biological organic fluorophores present.

The systems and techniques of the present invention can be characterized as discriminating between biological fluorescence and background pollution fluorescence, such as non-biological fluorescence.

In accordance with one or more embodiments, the present invention provides a method and system that employs the time emission decay profile, or fluorescence lifetime, to discriminate or characterize a sample of aerosol particles, in some cases or preferably, without the need for fluorescence wavelength information.

The systems and techniques of the invention can be characterized as providing a time resolved integrated laser induced fluorescence technique. For example and in accordance with one or more embodiments, the invention can provide a system and a method for using time-resolved light detection to discriminate between classes of fluorescing molecules to detect and, in some cases, count biological aerosol particles. The methods and systems of the present invention can classify sources of light according to arrival time at the detector. For example, very fast-arriving light, typically arriving less than about 0.1 nanoseconds (ns) relative to, typically the center, of an initiating emission, such as a laser pulse, can be classified as scattered light; fast-arriving light, typically arriving less than about 1 ns to about 7 ns, can be classified as having a biological fluorescence origin; and slow-arriving light, typically arriving greater than 7 ns, can be classified as fluorescence of a non-biological nature or origin. In some cases, because the processes can begin simultaneously, some of the scattered light can be fast fluorescence in nature and some of the fast fluorescence can be slow fluorescence. Accordingly, the systems and techniques of the present invention can correct for any overlap between such categories.

The present invention can be directed to tiered biological aerosol particle detection systems. For example, a first tier can comprise a fast, sensitive cue detector that typically operates, preferably continuously, to detect suspicious events. When such an event is detected, the fast detector typically cues a highly specific identification detector or detector array. Such a configuration can reduce false alarms without the expense and maintenance burden typically associated with continuously operating the specific identification detector. Thus, in accordance with one or more embodiments, the present invention can utilize time resolved induced fluorescence

techniques to detect suspicious events and cue one or more specific identification detectors.

In accordance with one or more embodiments, the systems and techniques of the present invention can detect natural, induced or resultant emissions, such as reflections or fluorescence of a sample comprising bioaerosol particles and resolve or deconvolve a response such as a composite time-dependent intensity into any one of a scatter component, non-biological component, and biological component. The measured intensity can be resolved into one or more non-biological components and, in some cases, one or more biological components.

The measurable emission can result naturally or be induced by an energy source. For example, aerosol particles can be excited to emit fluorescence by one or more electromagnetic radiation systems. The energy source can emit excitation energy in one or a spectrum of wavelengths. In accordance with one or more embodiments, the energy source 10 of the system of the present invention can comprise one or more electromagnetic radiation sources such as, but not limited to one or more lasers, as exemplarily shown in FIG. 2. Preferably, the excitation device, such as laser 10, can emit radiation, shown being transmitted through one or more optical fibers 12, with a pulse width sufficiently small that the scattering signal decay can be distinguished from a 1 ns emission decay profile. For example, a suitable pulse width can be less than about 5 ns and is preferably less than about 500 ps. The responses, such as a composite emission decay profile, typically scattered and/or emitted energy from the particles can be directed through one or more optical fibers 20 to devices to amplify and/or convert the response to one or more analyzable signals. For example, the response can be directed to a monochromator 22, a photomultiplier 24, and/or and oscilloscope 26. The signal can then be analyzed by, for example deconvolution, to identify components thereof in, for example computer 28. Computer 28 can further analyze the deconvolved signal into a discriminant vector, which can be mapped to provide a characterization of the biological/non-biological nature of the particles. The system can further comprise filter 32 to reduce any scatter component. As used herein, the term “discriminant vector” refers to the deconvolved or derived components of a response from an excited particle. Typically

each particle has an associated discriminant vector which can be compared by, for example, mapping to provide a characterization of the nature of the particle. For example, the discriminant vector can be mapped to provide an indication of a biological and/or non-biological aspect of the particle.

5 Optionally, a trigger signal 30 can be directed to, for example oscilloscope 26, to provide an index for initiation of analysis sequences.

 The laser light may interact with particles in a defined region of space and observed and/or a parameter thereof measured by a detector. The interaction region can be enclosed in a flow cell 14, which can prevent unwanted ambient particles and
10 unwanted ambient light from contamination or otherwise introducing unquantifiable interferences. Particles to be analyzed, from source 16, can be introduced into flow cell 14 through a small nozzle, to confine them to a well-defined interaction region where the excitation energy, such as a laser light, can be concentrated, and where the detection optics or optical devices can focus, for efficient collection of emissions.

15 Preferably, the particle stream is accompanied, more preferably, surrounded with an annular flow of particle-free air, which is typically referred to as sheath air 18. Sheath air 18 can further collimate the particle stream so that it can be confined in the interaction region and can prevent particle deposition on the optics of the system. More preferably, annular flows of the particle stream and the sheath air are combined
20 or flow isokinetically, with the same velocity, to reduce any turbulent mixing that may cause particles to be transported from the inner flow to the outer flow. Concave mirrors, spherical, parabolic, or elliptical, can be further utilized to reflect emitted energy, e.g., light, traveling away from the collection optics, so that it can travel toward and be captured by the collection optics.

25 As shown schematically in FIG. 3, flow cell 14 can have one or more excitation focusing devices such as focusing lens 36 that can direct the energy directed through fiber 12 to a particular desired region 42 to increase the likelihood of interaction with the particle or particles under analysis. Flow cell 14 can further
30 comprise one or more collection systems such as collection lens 40 that directs emitted response energy, e.g. composite emission decay profile, to fiber 20. Flow cell 14 can further comprise a beam dump 44, typically disposed distant from focusing

lens 36, to capture energy not absorbed or scattered. Further, flow cell 14 can comprise one or more retroreflectors 46 to facilitate direction of a response to collection lens 40.

Examples of suitable excitation devices include a SURELITE™ I quadrupled
5 YAG laser with a laser emission at 266 nm, available from Continuum, Santa Clara, California, a quadrupled YAG microchip laser with a laser emission at 266 nm, available from JDS Uniphase Corporation, San Jose, California; a nitrogen laser with an emission at 315 nm; a modulated diode laser system with a laser emission at 375 or 405 nm, available from Becker & Hickl GmbH, Berlin, Germany; and a tripled
10 Ti:Sapphire laser with tunable output in the ultraviolet regime.

In accordance with one or more embodiments, the systems and techniques of the present invention can comprise or utilize a suitable flow cell for detection of emitted light from an aerosol sample. The flow cell may comprise, for example, an enclosed space formed by the intersection of three tubes or boreholes or channels,
15 preferably, along three orthogonal axes. The excitation energy can be introduced along one axis by, for example, suitable optics or optical devices so that it can be concentrated in the interaction region. The detection optics can be placed along the second axis so that the emitted energy can be transmitted or reflected into one or more detectors. A concave retroreflector may be placed opposite the detector to increase
20 the light collection efficiency, preferably when a single detector is utilized. The airstream containing the particles, and optionally an annular flow of particle-free sheath air, can be introduced isokinetically along the third axis.

Any suitable detector can be utilized in the systems and techniques of the present invention to measure a composite emission decay profile. The detector can
25 measure a specific wavelength, a portion of the emitted spectrum, or, in some cases, the entire measurable spectrum. The detector should have a suitably rapid response time, for example less than 5 nanoseconds or preferably less than 500 picoseconds. Examples of suitable detectors include a model 1P28 photomultiplier tube, available from Hamamatsu Photonics, K.K., Hamamatsu City, Japan; a model APM-400
30 avalanche photodiode module available from Becker & Hickl GmbH, a model PMC-

100 photomultiplier module also available from Becker & Hickl GmbH; and a streak camera available from Hamamatsu Photonics, K.K.

In accordance with one or more embodiments of the invention, the signal representing the composite emission decay profile can be obtained by a spectroscopic method preferably having time resolution, such as 100 picoseconds (ps) to distinguish
5 different components of the decay. For example, a time-correlated single photon counting (TCSPC) technique may be utilized or other techniques that record low level light signals with, preferably, picosecond time resolution.

The signal, typically corresponding to a measured response to the initiating or
10 exciting energy can be represented as a signal, which can be sent to one or more analytical devices or system. Suitable devices or system components include a digitizing oscilloscope with minimum bandwidth 500 MHz such as a model TDS 3052 oscilloscope available from Tektronix, Inc., Beaverton, Oregon; a computer interface card, such as a general purposed interface board (GPIB), USB, or RS-232
15 interface; a computer preferably utilizing a PENTIUM[®]-based microcomputer or a “palmtop” or personal digital assistant computer; instrument control systems such as MATLAB,[™] IGOR PRO,[™] LABVIEW,[™] or other custom software and/or hardware; and waveform analysis such as MATLAB,[™] IGOR PRO,[™] SIGMAPLOT,[™] or other custom software or hardware. The analytical device can
20 evaluate the signal and decompose it into substituent components. Preferably, the device can utilize one or more decomposition techniques to identify a scatter component and, if present, a fluorescence component. More preferably, the device can also utilize techniques such as deconvolution to identify a non-biological component, and, if applicable, a biological component, of the composite response or
25 the fluorescence component thereof. In some cases, the response can comprise one or more scatter components and/or one or more fluorescence components. In still other cases, the fluorescence component can comprise one or more biologically-
corresponding or biological component and one or more nonbiologically-
corresponding or non-biological component. The deconvolution techniques can be
30 performed until derived results have sufficiently converged compared to the measured signal. Such convergence criteria can be tailored to particular requirements.

Signal decomposition techniques can be used to deconvolute the signal to obtain very fast, fast, and slow decays, each typically characterized by decay constants on the order of picoseconds, nanoseconds, and tens of nanoseconds, respectively. FIG. 4 shows deconvolved components from the total or composite response measured as a composite emission decay profile in FIG. 1. FIG. 4 exemplarily shows a total response signal 100 comprising a scatter component 102, typically associated with an exciting energy, and can be considered reflected, scattered energy from, for example, illuminated particles. In FIG. 4, the scatter component is shown with a Gaussian profile that may arise from the time profile of the excitation energy, e.g. the laser pulse. However, the scatter component will typically have the profile of the Instrument Response Function, discussed further below. The response can further comprise a biological component 104, typically having an exponential emission decay profile and a non-biological component 106, also typically having an exponential emission decay profile. As described, the non-biological component typically has a longer duration profile relative to the biological component. By separating the signal components according to their decay characteristics, the biological fluorescence can be distinguished from non-biological fluorescence and from scattered light. Thus, the present invention can provide systems and techniques that utilize signals that can be recorded with a single photodetector, without dispersion or filtering, e.g. by wavelength, of the signal.

However, a filter may be utilized, at the excitation wavelength, to reduce the scattered light intensity component, which can be advantageous because the scatter component typically has a greater magnitude than the magnitude or contribution attributable to biological and/or non-biological fluorescence. The filter may comprise a long-pass or band-pass filter, which, preferably, selectively compensates for the excitation wavelength.

The composite intensity decay profile can be characterized as a sum of terms including S , the scattered light pulse, and n fluorescence decay terms I_n . The scattered light pulse profile is typically influenced by the distribution of ray lengths from the excitation source to the detector, and may be considered sufficiently narrow that it may be assumed to have zero width, relative to elapsed time. Intensity decays can be

represented as $I_n = I_{o,n} e^{-(t/\tau_n)}$. Additionally, each term is typically convolved with the Instrument Response Function (IRF), which arises from the laser pulse shape and other aspects of the optical system and detector electronics. The IRF is determined via reflected or scattered light, where it is assumed that the only contribution the shape of a reflected or scattered light pulse is the IRF. This determined IRF is typically used during the deconvolution process.

A time constant τ_n can be respectively associated with each of the n biological and non-biological fluorescence decay components. Notably, one or more time constants, corresponding to one or more exponential profiles, can comprise each of the biological and the non-biological components.

Deconvolution of the different decays allows the fluorescence to be grouped into short and long lifetime bins or subcomponents. As exemplarily shown in FIG. 4, more than half of the total fluorescence (area under the curve) detected between about 1 ns to about 7 ns can be due to non-biological sources, such as PAH compounds, in the gas phase and/or adsorbed on bioaerosol particles. Deconvolution can be performed by utilizing statistical curve-fitting techniques to identify the scattering component, the non-biological component and the biological component. These statistical techniques typically construct a trial composite decay profile using initial guesses for the intensity and decay parameters. Initial guesses are based on physical expectations about the sample being characterized. The parameters are typically varied to minimize the difference between the constructed composite decay profile and the composite decay profile. The vector of parameters that reduces the difference between constructed and measured profiles below some predetermined tolerance, usually within a predetermined maximum elapsed time, is chosen as best representing the components of the measured composite decay profile. An example of a suitable algorithm for curve-fitting is the Levenberg-Marquardt method. Examples of software containing the Levenberg-Marquardt algorithm or other suitable curve-fitting algorithms include, but are not limited to, IGOR PRO,TM SIGMAPLOT,TM MATLAB,TM and FLUOFITTM as disclosed by, for example, J. Enderlein and R. Erdmann in "Fast Fitting of multi-exponential decay curves", Optics Communications 134(1-6), 1997, pp. 371-378.

The intensities corresponding to the scatter, total biological fluorescence, and total non-biological fluorescence may be determined by summing all intensities for components with lifetimes within a certain range. For example, biological fluorescence could be taken as the sum of all intensities for components with lifetimes between about 0.1 and about 7 ns. Likewise, non-biological fluorescence could be taken as the sum of all intensities for components with lifetimes greater than about 7 ns. However, the lifetime ranges used to classify emission as scatter, biological fluorescence, or non-biological fluorescence may be chosen based on one or more factors including physical insights about the system being measured, lifetimes published in the scientific literature, and laboratory measurements of test particles. In some cases, the classification separation between biological and non-biological fluorescence can be varied as necessary to accommodate region or environment specific requirements. Thus, the biological components can be classified as those having time constants between about 0.1 ns to about 7 ns and, correspondingly, non-biological components can be classified as those having time constants greater than about 7 ns.

The total scatter and fluorescence intensities can thus define a discriminating vector comprising n-dimensional components corresponding to one or more of the scatter component, the biological components, and the non-biological components. Typically, the discriminating vector provides a characterization of the nature of the sampled aerosol particles in a three-dimensional map.

In some embodiments of the invention, the fluorescence intensities can be normalized by dividing by the scatter value. This can reduce the number of vector components by a degree of freedom to, for example, two, so a two-dimensional map can be used to provide a characterization of the nature of the analyzed sample of aerosol particles.

For example, once the decay rates of the different signal components have been characterized, the corresponding, associated initial response values may be plotted on a map that aids in discriminating between biological and non-biological signatures. FIG. 5 shows an example of where various aerosol types may be found on a map comparing normalized fluorescence intensities and scattering intensity. As

exemplarily shown in FIG. 5, toward the right side of the map, the fast intensity component, typically associated with biological fluorescence can be equal to or greater than the slow intensity, which indicates that biological species are probably present. In some cases, scattering intensity can be represented by the size of the spot; if large, it can indicate a large particle size. Scatter intensity may be used, as is done with, for example, BAWS Tier III, as a proxy for size, so that intense fluorescent scattering species are probably large pollen grains, while very weak fluorescent scattering species may be submicron soot aerosols or fragments of bioparticles. Measurements of known aerosol types may be utilized to populate such maps and, preferably, provide delineating boundaries between biological and non-biological aerosols.

Other methods of analyzing the data to produce classification criteria can be utilized in accordance with the systems and techniques of the present invention. For example, Fourier transformation of the time domain data can yield a spectrum of decay frequencies that can be associated with the decay times. It is also possible to characterize particles based on the ratio of non-biological fluorescence to biological fluorescence, with or without normalization to scattering. Further, maps similar to that presented in FIG. 5 may be generated for other classification criteria, see for example FIG. 8, which is discussed in the examples.

In some cases, it is possible to combine the time-resolved detection method with other techniques such as those pertinent to dispersed or filtered fluorescence, to obtain both time and spectral information about the measured response. This can yield additional information about the fluorescing species or molecules. For example, the manner by which the fluorescence spectrum changes over time may indicate spectral relaxation, which can be indicative of how quickly a molecule's environment adapts to photonically induced changes in the molecule's electric field. Spectral relaxation can be dependent on the viscosity and polarity of the molecule's environment; thus, it may be a way of differentiating a molecule adsorbed on a solid surface, from a molecule embedded in a biological membrane, from a molecule in a liquid environment, e.g. cellular cytoplasm. This may allow detailed identification of

classes of biological agents, because, it is believed, bacterial spores typically have little or lower water relative content.

Aerosol particles, entrained in airflow, can be excited, for example, one at a time, by pulsed laser radiation, light, at a wavelength that produces fluorescence from biological fluorophores such as tryptophan, tyrosine, NADH, or flavin compounds. Said particles also scatter said radiation to produce a scattered light pulse. Both fluorescence and scattered light can be detected by the same detector. This produces a signal pulse similar to that shown in FIG. 4. The measured signal corresponding to a response can comprise scattered light components and one or more of particle-bound biological fluorophore components and particle-bound, non-biological organic fluorophore components, and, in some cases, gas phase, non-biological organic fluorophore components, in the excited or illuminated focal region.

In accordance with one or more embodiments of the invention, the signal can be obtained by sampling at predetermined and/or strategic intervals using, for example, a spectroscopic method to distinguish different components of the decay. For example, a suitable method can comprise time-gated photon counting, but other methods may also be suitable.

Preferably, the excitation energy, e.g. laser beam, has a pulse width sufficiently small that the scattering signal decay can be distinguished from a 1 ns emission decay profile. A suitable pulse width can be about less than about 500 ps.

The gate start times and gate widths are chosen to sample the light intensity at times when most of the light is due to one source or another. FIG. 6 shows how gate times can be selected. The signals can be considered to be corresponding components exemplarily shown in FIG. 4, labeled as very fast scatter component 102, fast biological fluorescence component 104, and slow non-biological fluorescence component 106. As exemplarily shown, the signal traces can be offset from zero for clarity. The gate pulse is shown in the bottom trace, where a high gate signal corresponds to a period during which the detector is on or activated, and a low value corresponds to a period during which the detector is off or inactive. FIG. 6 exemplarily shows three panes to indicate events occurring on different time scales. For example, in (C), the gates, set at about 10 ns, 20 ns, and 30 ns, receive response

measurements associated with long-lived, typically non-biological, fluorescence. Fluorescence intensities at such points may thus be used to estimate the contribution from non-biological fluorescence. In (B), gates, set at about 1 ns, 2 ns, and 5 ns, receive response measurements can be associated with long-lived fluorescence, which would preferably be subtracted based on the preceding analysis pertinent to long-lived, typically non-biological, fluorescence, and/or short-lived, typically biological, fluorescence. In (A) at a time from about -0.5 ns to about 0 ns, after compensating for estimated fluorescence, as determined above, the remaining detected light can be attributed to scattering of the exciting energy, e.g., the laser. Gate activation periods can be relative to the center of an excitation energy discharge but can be measured relative to the trigger that initiates the excitation energy discharge. Gate positions can be optimized based on data from environmental and test aerosols.

The three measured categories can then be used to map the data as shown in FIG. 5. Likewise, the position on the plot can be indicative of the nature of the sampled aerosol particles, e.g., whether the fluorescence is biological, non-biological, or both. Other mapping techniques can utilize ratios of short and long lifetime fluorescence components relative to the scatter component and provide a two-dimensional map as well as computing the ratio of short-lifetime fluorescence to long-lifetime fluorescence and plotting the ratio relative to scatter to also provide a two-dimensional characterization of the nature of the particles. Further, statistical and/or geometric techniques can be utilized to, for example, assign probabilities as to the nature or likelihood of biological or non-biological character of the particles. For example, statistical techniques can be utilized to assign a probability or likelihood that the particle is or comprises a target microorganism. Likewise, geometrical techniques can be utilized to assign distances representative of the character of the particle relative to one or more categories. For example, separation distances can be determined for a measured, analyzed discriminant vector relative to vectors of one or more known particles. The relative separations can thus be viewed as a likelihood of presence, likelihood of result, and/or likelihood of contribution.

The functions and advantages of these and other embodiments of the invention can be further understood from the examples below. The following examples

illustrate the benefits and advantages of the systems and techniques of the invention but do not exemplify the full scope of the invention.

Example 1. Prophetic Characterization System.

5 Prophetic data can be generated for several types of particles; non-fluorescent particles (scattered light only); particles containing a mixture of common atmospheric PAHs having representative lifetimes about 15, about 22, and about 30 ns; hazardous bioaerosols (respirable bioparticles) having a representative lifetime of about 2 ns; background bioaerosols (e.g., a pollen grain) having a typical lifetime of about 2 ns.

10 This prophetic example data is constructed to approximate the results expected from one example implementation of the present invention. The experimental system can comprise a quadrupled SURELITE I™ YAG laser emitting at 266 nm available from Continuum, Inc., and a flow cell comprising about two-inch cubic aluminum block bored through on three orthogonal axes. Aerosol particles are introduced
15 isokinetically within an annular, particle-free sheath flow, wherein the aerosols interact with the emitted laser energy in a central interaction region. Emitted radiation from the sample of aerosol particles or reflected by a retroreflector is collected by a collection optical system. Excess laser light that is not absorbed or scattered by the sample of aerosol particles is captured by a beam dump disposed distant from a laser
20 focusing lens. A silica/silica optical fiber cable conducts the emitted laser energy to the cell and a second silica/silica optical fiber conducts the response from the cell to the detector, both optical fibers are model FVA available from Polymicro Technologies, LLC, Phoenix, Arizona. Optionally a monochromator, such as those available from Jarrell Ash Corp./Thermo Electron Corp., Woburn, Massachusetts, or
25 other similar device can be utilized to select a single emission wavelength for detection. The system can further comprise one or more photomultiplier modules such as a model 1P28 photomultiplier tube available from Hamamatsu Photonics, K.K., Hamamatsu City, Japan; a model TDS 5032 digitizing oscilloscope available from Tektronix, Inc., Beaverton, Oregon, to enhance or amplify the response; a
30 computer comprising a PENTIUM® microprocessor with a general purpose interface board (GPIB) running LABVIEW™ software, available from National Instruments

Corporation, Austin, Texas, to control the system and/or record and analyze data. Data analysis can be performed utilizing commercially or otherwise freely available software from for example MATLAB™ available from MathWorks, Inc., Natick, MA and/or FLUOFIT™ software for deconvolving composite emission decay profiles by performing, for example, multi-exponential least squares fitting.

The specific hardware configuration chosen to make the fluorescence measurements determines the Instrument Response Function (IRF). The IRF is a temporal function that alters the expected exponential decay profiles in a manner equivalent to mathematical convolution. Therefore, if the IRF for a given experimental configuration is known, it is possible to predict the approximate form of the signal that will be recorded from a particle of specified size and composition.

Further, the IRF for a given experimental configuration can be recorded by measuring the time-dependent intensity profile of a light pulse reflected from a mirror or any convenient, non-fluorescing surface. Therefore, it is possible to construct a prophetic data set relating to a particle of specified size and composition, as measured by a spectrometer of specified hardware configuration. The basic component of a time-domain fluorescence signal is an exponential decay, $Ie^{(-t/\tau)}$, where I is the intensity and τ , the fluorescence lifetime. Individual signals for scattered light, and fluorescence with lifetimes characteristic of biomolecules and common PAHs, are summed to construct the ideal decay profile. The recorded IRF for the spectrometer in use is convolved with the ideal decay profile to produce a prophetic decay profile for the specified particle and experimental system.

Example 2. Analysis of a Prophetic Response.

FLUOFIT™ software was used to analyze a convolved representative response to derive up to three exponential decay components and one scatter component. The resultant of this was a set of intensities and lifetimes that characterize different components of the decay. Intensities for short-lived fluorescence were summed and taken as representative of biofluorescence. Intensities for long-lived fluorescence were summed and taken as representative of PAH fluorescence. The IRF intensity was taken as representative of scattered light, which

is typically related to particle size. The short- and long-lived fluorescence totals and scattered light total were used to locate the particle on a three-dimensional map to classify the various particles.

Table 1 lists exponential decay parameters of representative species that may be encountered. For PAHs, the “relative importance” (RI) is a measure of the importance with respect to fluorescence measurements, compared to biomolecules. The calculation was performed as follows: published measurements of concentration in atmospheric gas/particulate phase were used to estimate gas or surface concentration of the PAH in question. Particles sizes of 2 μm diameter were utilized. Fluorescence emitted by the PAH was calculated based on the above concentration, multiplied by the absorption cross section and fluorescence quantum yield. The total fluorescence emitted from a 2 μm *Bacillus Globigii* (BG) spore was estimated based on measurements from several laboratories.

PAH fluorescence was normalized relative to BG spore fluorescence to give the RI score. Of the 39 compounds found in the atmosphere by one environmental study, only five have RI of 0.1 or more. Of these, all but two have lifetimes longer than expected for bioparticles.

Representative exponential decay parameters were determined. The values used in this prophetic dataset relate to the Relative Importances and Lifetimes (listed in Table 1) and are listed in Table 2.

Five particle signals were constructed and listed in Table 3. The first particle representation corresponds to a dust grain having no fluorescence aspect. The second particle representation corresponds to a 2 μm diameter particle having PAH #1, 2, and 3 aspects. The third particle representation corresponds to a 2 μm diameter spore having a fluorescence time constant of about 2 ns. The fourth particle representation corresponds to a 20 μm diameter pollen with a fluorescence time constant of about 2 ns. The fifth particle representation corresponds to a microbial spore contaminated with PAH 1 and 3.

Table 1. Known atmospheric gas phase or particulate fluorophores along with estimated time constants (presented as lifetimes) as well as their estimated importance relative to BG fluorescence.

Aerosol Species	Relative Importance	Lifetime (ns)
Phenanthrene (gas phase)	1.5	57.5
Phenanthrene (particle)	1.5	57.5
<i>B. Globigii</i> (2 μ m dry spore)	1.0	2
Fluorene (particle phase)	0.8	10
Fluorene (air phase)	0.6	10
Naphthalene (particle phase)	0.4	96
C1-C4 Anthracenes (gas phase)	0.4	<6
C1-C4 Anthracenes (particle phase)	0.3	<6
Anthracene (particle phase)	0.1	<6

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Table 2. Representative model fluorophores and scattering sources along with typical time constants (presented as lifetimes) and intensities in arbitrary units. These constituents were used to construct the prophetic example signals.

Compound Name	Intensity (arbitrary units)	Tau, t (ns)
PAH #1 (phenanthrene)	150	57.5
PAH #2 (fluorine)	80	10
PAH #3 (C1-C4 anthracene)	40	5
Microbial Spore	100	2
Pollen Grain	10,000	2
Scatter from 2 μ m particle	100	0
Scatter from 20 μ m particle	10,000	0
Scatter from 100 μ m particle	250,000	0

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FIGS. 7A-7E show constructed decay profiles for each of these particles.

FIG. 7A shows the constructed decay profile for the first particle, the dust grain. FIG. 7B shows the constructed decay profile for the second particle, a mixture of PAH 1, 2 and 3 on a 2 μ m diameter particle. FIG. 7C shows the constructed decay profile for the third particle, microbial spore. FIG. 7D shows the constructed decay profile for the fourth particle, pollen. FIG. 7E shows the constructed decay profile for the fifth particle, spore with PAH 1 and 3 contaminations.

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Table 3. Constructed particle description.

Particle (Description)	Size (μm) Scatter Intensity	Fluorescent Intensity	Lifetimes (ns)
1 (Non-fluorescent dust grain)	100 2,500,000	None	None
2 (Mixture of PAH 1, 2 and 3)	2 1,000	150, 80, 40 respectively	57.5, 10, 5 respectively
3 (Microbial Spore)	2 1,000	100	2
4 (Pollen Grain)	20 100,000	10,000	2
5 (Microbial/PAH 1 and 3)	2 1,000	150, 40, 100 respectively	57.5, 5, 2 respectively

The decay profiles shown in FIGS. 7A-7E were deconvolved with
5 multiexponential, least squares fit to derive intensity and lifetime of each decay component.

Table 4 lists the derived results. As shown in Table 4, for each of the
constructed decay profiles, the derived Fit Percentage (which is representative of the
initial intensity) closely corresponded to the Actual Percentage for each of the
10 components of each particle. Likewise, the derived Fit Lifetime closely corresponded
to Actual Lifetime. For example, for particle 1, which was a dust grain having a
scatter component and no fluorescence component, the derived Fit Lifetime was about
0.003, indicative of no decay component, no fluorescence component.

For particle 3, the deconvolution process identified a scatter component and a
15 fluorescence component, the fluorescence component classified as biological because
it had a lifetime (Fit Lifetime) of less than about 7 ns. The scatter component was
derived to be about 91 % (as Fit Percentage), closely corresponding to the Actual
Percentage (91 %). The fluorescence component was derived to have a Fit Percentage
(8.7 %) close to the Actual Percentage (9 %). The derived Fit Lifetime (1.5 ns) also
20 corresponded closely to the Actual Lifetime (2 ns). Thus, the results presented in
Table 4 show that various prophetically constructed particles can be characterized by,
for example, deconvolution, to provide components of a response from the particle.

Table 4. Deconvolution results.

Particle	Component	Actual Intensity	Actual Percentage	Actual Lifetime	Fit Percentage	Fit Lifetime	Intensity error	Lifetime Error
1	Scatter	2,500,000	100	0	100	0.003	0	0.003
2	Scatter	1,000	79	0	88	0.04	9	0.04
	PAH #1	150	12	57.5	6.2	57.5	-5.8	0
	PAH #2	80	6	10	3.9	9.86	-2.1	0.14
	PAH #3	40	3	5	0	4.77	-3	0.23
	Total	1,270						
3	Scatter	1,000	91	0	91.3	0.04	0.3	0.04
	Bio	100	9	2	8.7	1.5	-0.3	0.5
	Total	1,100						
4	Scatter	100,000	91	0	91.3	0.04	0.3	0.04
	bio	10,000	9	2	8.7	1.5	-0.3	0.5
	Total	110,000						
5	Scatter	1,000	78	0	86	0	8	0
	PAH #1	150	12	57.5	6	57.5	-6	0
	PAH #3	40	3	5	2.2	4.9	-0.8	0.1
	Bio	100	8	2	5.9	1.95	-2.1	0.05
		1,290						

Example 3. Mapping Particle Characteristics.

In this example, particle characteristics as represented by a discriminant vector were mapped according to their position in time-resolved fluorescence signal space.

FIG. 8 is a map showing the relative positions of each of the constructed particles analyzed in Example 2 with respect to a scatter component, a non-biological fluorescence component, and a biological fluorescence component. The discriminant vectors for each of the dust grain 1, PAH mixture 2, spore 3, pollen 4, and spore with PAH 5 were mapped.

As shown, the spatial groupings provided an indicating of the general composition of particle. Thus, the technique of mapping can be utilized to facilitate the characterization of the nature of particles based on the particle's deconvolved response. Other representative discriminant vectors have also been shown for comparison.

As discussed above, other mapping techniques can be utilized to characterize the nature of each particle. For example, it may be possible to compute the ratios of short- and long-lifetime fluorescence to scatter, and plot ratios in two dimensions or to compute the ratio of short-lifetime fluorescence to long-lifetime fluorescence, and plot the ratio relative to scatter in two dimensions. It may also be possible to analyze groupings using statistical and geometrical algorithms, without using a graphical representation.

Having thus described several aspects of at least one embodiment of this invention, it is to be appreciated various alterations, modifications, and improvements will readily occur to those skilled in the art. Such alterations, modifications, and improvements are intended to be part of this disclosure, and are intended to be within the spirit and scope of the invention. For example, one or more detectors can be utilized in the systems and techniques of the present invention and, in accordance with some embodiments, a detector may be utilized or configured to measure a component of a composite emission decay profile; and in some cases, a second, typically separate detector can be utilized to measure a second component of the composite emission decay profile. Moreover, the time boundaries cited herein are approximate, typically based on the scientific literature, and may be adjusted and optimized for a variety or

particular measurement situation. Further, the present invention has been described as characterizing an aerosol particle but need not be limited as such. Thus, one or more particles may be characterized, which can be airborne or otherwise. Accordingly, the foregoing description and drawings are by way of example only.

5 What is claimed is: